

TITLE OF THE INVENTION

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Optical Measurement Apparatus for Living Body and
Method Thereof

FIELD OF THE INVENTION

5 [0001]

The present invention relates to an optical measurement apparatus for living body, in particular, an optical measurement apparatus for living body having an improved function of evaluating whether the settings 10 of respective optical fiber probes of a probe device, which is attached to an inspection area of a subject, are adequate and which permits to evaluate correctly whether the settings of the respective optical fibers on a body surface of the subject, and a method thereof.

15 BACKGROUND ART

[0002]

An optical measurement apparatus for living body is an apparatus which permits to measure simply and easily living body information inside a living body, 20 for example, such as blood circulation, hemodynamics and variation of hemoglobin concentration with low restriction to a subject and in a non-invasive manner to the living body through irradiating light having frequencies of from visible to near infrared regions 25 to the living body and detecting the light penetrating through inside the living body.

[0003]

When performing an optical measurement for living body of a subject representing a living body with the optical measurement apparatus for living body, at first an optical fiber probe device including irradiation use optical fiber probes and light receiving use optical fiber probes which are arranged alternatively at respective lattice points of, for example, 4x4 is attached on an inspection area of the subject, for example, on the head portion. In the case of the optical fiber probe device including irradiation use optical fiber probes and light receiving use optical fiber probes which are arranged alternatively at respective lattice points of 4x4, a total of 24 measurement channels each including a measurement point between respective adjacent irradiation use optical fiber probes and light receiving use optical fiber probes are formed inside the living body of the subject.

[0004]

Figs.2~5 are diagrams showing schematically four manners of settings of mutually adjacent irradiation use optical fiber and light receiving use optical fiber which are set on a body surface of a living body representing a subject and between which a measurement channel including a measurement point is formed.

[0005]

Fig.2 is an example where the setting of the optical fibers is adequate and shows a state in which

inspection light 203 irradiated from irradiation use optical fiber 201 passes through inside of living body 205 and light 204 emerged outside from the living body makes incident into light receiving use optical fiber 202. Under this optical fiber setting condition, a sufficient near infrared light, which is subjected to absorption and reflection by hemoglobin inside the living body can be detected.

[0006]

Fig.3 is an example where the setting of the irradiation use optical fiber is inadequate and shows a state in which inspection light 303 irradiated from an irradiation use optical fiber 301 passes through an obstacle 306 such as hair, light 307 of which intensity is weakened passes through inside living body 305 and penetrating light 304 emerged outside from the living body makes incident into light receiving use optical fiber 302. Under this optical fiber setting condition, since signals of the irradiation light 303 are disturbed by the obstacle 306, sufficient near infrared light subjected to absorption and reflection by hemoglobin inside the living body 305 can not be detected. Further, even in a case when no obstacle 306 such as hair is caught between the irradiation use optical fiber 301 and the surface of the living body, if the irradiation use optical fiber 301 is remote from the surface of the living body and the attenuation of the irradiation light

is extreme, since sufficient inspection light which has penetrated through the subject can not be detected, the setting of the optical fiber is evaluated as inadequate.

[0007]

5 Fig.4 is an example where the setting of the light receiving use optical fiber is inadequate and shows a state in which irradiation light 403 irradiated from an irradiation use optical fiber 401 passes through inside living body 405 and penetrating light 404 emerged
10 outside from the living body passes through an obstacle 406 such as hair, light 407 of which intensity is weakened makes incident into light receiving use optical fiber 402. Under this optical fiber setting condition, since signals of the penetrating light 404
15 are disturbed by the obstacle 406, sufficient near infrared light subjected to absorption and reflection by hemoglobin inside the living body 405 can not be detected. Further, even in a case when no obstacle 406 such as hair is caught between the light receiving use
20 optical fiber 401 and the surface of the living body, if the light receiving use optical fiber 402 is remote from the surface of the living body and the attenuation of the irradiation light is extreme, since sufficient inspection light which has penetrated through the
25 subject can not be detected, the setting of the optical fiber is evaluated as inadequate.

[0008]

Fig.5 is an example where the setting of both irradiation use and light receiving use optical fibers is inadequate because both are inadequately remote from a living body representing a measurement object and 5 shows a state in which since irradiation use optical fiber 501 is remote from a living body, irradiation light 503 of which intensity is weakened passes through inside living body 505 and penetrating light emerged outside from the living body of which intensity is 10 weakened makes incident into light receiving use optical fiber 502. On the other hand, since the light receiving use optical fiber 502 is also remote from the surface of the living body, light from the irradiation use optical fiber 501 of which intensity is high in 15 comparison with that of the light passed through inside the living body is directly makes incident to the light receiving use optical fiber 502. Under this condition, since the penetrating light 504 passed through inside the living body 505 mixes with the direct light 506 from 20 outside the living body, the amount of received light is much, however, sufficient near infrared light which is subjected to absorption and reflection by hemoglobin inside the living body 505 representing measurement object can not be detected.

25 [0009]

In a conventional optical measurement apparatus for living body as, for example, disclosed in

JP-A-11-311599, an evaluation and judgment is performed whether the setting of respective pairs of adjacent optical fibers each constituting a measurement channel of a probe device which is attached on a body surface of an inspection area of a subject is adequate or not in such a manner that after setting the respective optical fibers, a short time preparatory measurement is performed prior to beginning an actual measurement, in which gains of irradiation light amount from respective irradiation use optical fibers and received light amount of respective paired light receiving use optical fibers are detected, more specifically, a gain adjustment is performed for the respective measurement channels and for a measurement channel of which gain adjustment has failed the setting of the optical fibers is evaluated and judged as inadequate and resetting work of the optical fibers is performed for the respective concerned channels.

[0010]

However, with the method as disclosed in the conventional optical measurement apparatus for living body, the inadequate optical fiber setting state as shown in Fig.5 was evaluated and judged as adequate optical fiber setting because the amount of light received by the light receiving use optical fiber is sufficient, although the amount of light penetrated inside the living body containing hemoglobin signals

is insufficient.

[0011]

For this reason, even though the measurement data of such measurement channels is erroneous measurement data, the erroneous measurement data are treated as correct measurement data, operated and processed, of which result possibly causes an erroneous diagnosis or reduction of diagnosis efficiency.

[0012]

10 An object of the present invention is to provide an optical measurement apparatus for living body having a function which performs a correct evaluation and judgment whether the setting of respective pairs of adjacent optical fibers each constituting a measurement channel of a probe device which is attached on a body surface in an inspection area of a subject is adequate or not and a method thereof.

[0013]

Another object of the present invention is to 20 provide an optical measurement apparatus for living body, which can prevent an erroneous diagnosis or reduction of diagnosis efficiency due to an inadequate setting of respective pairs of adjacent optical fibers each constituting a measurement channel of a probe 25 device which is attached on a body surface in an inspection area of a subject and a method thereof.

SUMMARY OF THE INVENTION

[0014]

An optical measurement apparatus for living body according to the present invention being provided with a light irradiation means including an irradiation use optical fiber which irradiates light subjected to different modulation from a light irradiation position to a living body, a light detection means including a light receiving use optical fiber which detects light penetrated inside the living body at a detection position and outputs an electrical signal corresponding to the amount of light detected at a measurement portion which is determined in relation to the light irradiation position, a signal processing means which calculates hemoglobin concentration at every measurement portion based on the electrical signal from the light detection means and display means which displays a calculation result of the signal processing means, is characterized in that the signal processing means includes an evaluation and judgment means which evaluates and judges an intensity of pulse wave contained in the hemoglobin signals and performs an evaluation and judgment of adequacy of the setting state of the irradiation use and/or light receiving use optical fiber on the body surface of the living body based on the evaluation and judgment.

[0015]

Further, the evaluation and judgment means

according to the present invention is characterized by performing the evaluation and judgment based on the peak magnitude of a center frequency in the statistic of the hemoglobin signal.

5 [0016]

With the optical measurement apparatus for living body according to the present invention, an adequacy of the setting state of the irradiation use and/or light receiving use optical fiber on the body surface of the 10 living body can be correctly evaluated and judged.

[0017]

With the optical measurement apparatus for living body according to the present invention, since a possible mixture of erroneous measurement data from a 15 measurement channel constituted by a pair of inadequately set irradiation use and light receiving use optical fibers of the probe device is eliminated, an erroneous diagnosis or reduction of diagnosis efficiency can be prevented.

20 BRIEF DESCRIPTION OF THE DRAWINGS

Fig.1 is a block diagram showing a schematic constitution of an optical measurement apparatus for living body according to the present invention.

Fig. 2 is a view for explaining a manner of 25 attenuation of inspection light from an irradiation use optical fiber to a light receiving use optical fiber at a measurement channel when the irradiation use

optical fiber and the adjacent light receiving use optical fiber are adequately set on a body surface of a living body representing a subject.

Fig. 3 is a view for explaining a manner of
5 attenuation of inspection light from an irradiation use optical fiber to a light receiving use optical fiber at a measurement channel when the irradiation use optical fiber and the adjacent light receiving use optical fiber are inadequately set on a body surface
10 of a living body representing a subject, in that the irradiation use optical fiber is set remote from the body surface of the living body as well as hair is caught therebetween.

Fig. 4 is a view for explaining a manner of
15 attenuation of inspection light from an irradiation use optical fiber to a light receiving use optical fiber at a measurement channel when the irradiation use optical fiber and the adjacent light receiving use optical fiber are inadequately set on a body surface
20 of a living body representing a subject, in that the light receiving use optical fiber is set remote from the body surface of the living body as well as hair is caught therebetween.

Fig. 5 is a view for explaining a manner of
25 attenuation of inspection light from an irradiation use optical fiber to a light receiving use optical fiber at a measurement channel when the irradiation use

optical fiber and the adjacent light receiving use optical fiber are inadequately set on a body surface of a living body representing a subject, in that both irradiation use optical fiber and light receiving use optical fiber are set remote from the body surface of the living body.

Fig.6 is a flowchart for explaining a sequence in an embodiment for evaluating setting adequacy of respective pairs of irradiation use optical fibers and light receiving use optical fibers set on the body surface of a living body representing a subject, which is executed in a signal calculation and processing unit of an optical measurement apparatus for living body according to the present invention.

Fig.7 is a graph showing oxyhemoglobin variation signal calculated according to step 601 in Fig.6 at a certain channel for which the irradiation use optical fiber and/or the light receiving use optical fiber are adequately set.

Fig.8 is a graph showing oxyhemoglobin variation signal in a frequency band containing pulse wave due to heartbeat extracted by applying an HPF (high frequency band pass filter) to the oxyhemoglobin variation signal as shown in Fig.7 according to step 602 in Fig.6.

Fig.9 is a graph showing signal intensity $P(f)$ determined for respective frequencies by performing

frequency analysis on the oxyhemoglobin variation signal as shown in Fig.8 according to step 603 in Fig.6.

Fig.10 is a graph showing oxyhemoglobin variation signal calculated according to step 601 in Fig.6 at 5 another channel for which the irradiation use optical fiber and/or the light receiving use optical fiber are inadequately set.

Fig.11 is a graph showing oxyhemoglobin variation signal in a frequency band containing pulse wave due 10 to heartbeats extracted by applying an HPF (high frequency band pass filter) to the oxyhemoglobin variation signal as shown in Fig.10 according to step 602 in Fig.6.

Fig.12 is a graph showing signal intensity $P(f)$ 15 determined for respective frequencies f by performing frequency analysis on the oxyhemoglobin variation signal as shown in Fig.11 according to step 603 in Fig.6.

Fig.13 is a flowchart for explaining a sequence in an embodiment of optical measurement for living body 20 with an optical measurement apparatus for living body according to the present invention having a function of evaluating a setting adequacy of optical fibers for the respective measurement channels as shown in Fig.6 embodiment.

25 Fig.14 is a flowchart for explaining a sequence in another embodiment of optical measurement for living body with an optical measurement apparatus for living

body according to the present invention having a function of evaluating a setting adequacy of optical fibers for the respective measurement channels as shown in Fig.6 embodiment.

5 Fig.15 is a flowchart for explaining a sequence in still another embodiment of optical measurement for living body with an optical measurement apparatus for living body according to the present invention having a function of evaluating a setting adequacy of optical
10 fibers for the respective measurement channels as shown in Fig.6 embodiment.

BEST MODES FOR CARRYING OUT THE INVENTION

[0019]

Herein below, embodiments of the present invention
15 will be explained in detail. Fig.1 is a constitutional diagram of an optical measurement apparatus for living body according to the present embodiment. An optical measurement apparatus for living body 100 is constituted by an optical measurement unit for living body 101 and an optical signal for living body calculation and display unit 108, the optical measurement unit for living body 101 includes a laser generation unit 102 which generates near infrared light having frequencies of about 600~1200nm which easily
20 penetrates through a human body, a fiber unit 103 which guides and irradiates the laser beam generated from the laser generation unit 102, for example, toward a scalp
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portion, another fiber unit 103' which receives and detects the near infrared light subjected to absorption and reflection by hemoglobin at the brain surface, a probe 104 for attaching the fiber units 103 and 103'
5 to the head portion, an avalanche diode 105 for converting the inputted near infrared light into electrical signals, a lock-in amplifier 106 for amplifying the electrical signals and a continuously variable amplifier 107, and the optical signal for
10 living body calculation and display unit 108 is constituted by a memory 109 for recording the electrical signals from the continuously variable amplifier 107, a central processing unit CPU 110 for converting the electrical signals into hemoglobin signals, a hard disk
15 111 for recording the hemoglobin signals and a monitor 112 for displaying the hemoglobin signals.

[0020]

In addition to a hemoglobin signal calculation unit 113, which is provided conventionally, the central
20 processing unit CPU 110 includes a pulse wave calculation unit 114 which calculates pulse wave components due to heartbeats and a setting evaluation unit 115 which evaluates and judges setting adequacy of each pair of an irradiation use optical fiber and
25 a light receiving use optical fiber set at both ends of respective measurement channels, both of which are for realizing the present invention.

[0021]

Now, a sequence of evaluating adequacy of a setting state of an irradiation use optical fiber and/or a light receiving use optical fiber on a surface of a living body representing a subject as explained, for example, with reference to Fig.2~Fig.5, which is performed with the optical measurement apparatus for living body according to the present invention provided with the pulse wave calculation unit 114 and the setting evaluation unit 115, will be explained according to Fig.6 flowchart which is one embodiment of the present invention.

[0022]

At first, at step 601, for example, oxy-Hb values due to hemoglobin oxidation of respective measurement channels for every measurement are determined from the measurement result of the optical measurement for living body. In the present embodiment, although the oxy-Hb values are used, deoxy-Hb values due to deoxidation or total-Hb values relating to total hemoglobin can be used.

[0023]

Subsequently, at step 602, in order to extract pulse wave components due the heartbeats, a HPF (High frequency band Pass Filter) using a proper frequency value performed by a program provided in the pulse wave calculation unit 114 is applied to the measurement

result. Although the HPF (High frequency band Pass Filter) is usually used for the purposes of extracting pulse wave components due the heartbeats and of removing a low frequency band containing target components of 5 the optical measurement for living body, when a component different from the pulse wave component due to heartbeats is contained in the high frequency band, for example, when mixing of noises having a specific frequency is presumed, an LPF (Low Frequency band Pass 10 Filter) or a BPF (Band Pass Filter) performed by a program provided in the pulse wave calculation unit 114 is used. When the subject is a newborn, the frequency component used for the HPF is, for example, 1Hz. This is because when a subject is a newborn, the pulse wave 15 component due to heartbeats appears in a frequency band of 1.6~2.1Hz and in a frequency band below 1Hz living body information inside the living body (for example, such as functional signal representing hemoglobin concentration variation at a specific portion in the 20 brain caused by moving a part of the human body) which is the primary target of the measurement appears. Therefor, in order to extract pulse wave components due the heartbeats it is proper to use a HPF of 1Hz. Further, when the subject is an adult, it is proper to use a HPF, 25 for example, of 0.5Hz. However, a band threshold value (which frequency is to be used) for the band pass filter (such as HPF and LPF and a combination thereof) can be

arbitrarily input by an operator via an input unit (not shown).

[0024]

After extracting from the measurement result
5 signal components in the frequency band which are presumed as containing the pulse wave components due the heartbeats at step 602, a frequency analysis is performed with a program provided in the pulse wave calculation unit 114 at step 603 and the signal
10 intensity $P(f)$ for the respective frequency components f is calculated. Then, at step 604 a frequency having the maximum signal intensity among the signal components in the frequency band which are presumed as containing the pulse wave components due the heartbeats
15 is detected as a center frequency f_0 from the result of performing the frequency analysis.

[0025]

Subsequently, at step 605 a fourth order statistic K_{f0} around the detected center frequency f_0 and as shown
20 in the drawing is calculated and used as a parameter for judging the setting adequacy of optical fibers. The fourth order statistic K_{f0} represents the peak steepness of the signal intensity at the center frequency f_0 and when pulse wave signals due to
25 heartbeats are contained many, the value becomes large and when pulse wave signals due to heartbeats are contained less, the value becomes small. Therefore, if

the setting of the optical fibers is adequate, since the light used for the measurement passes inside the living body, in particular, through a blood vessel and makes incident to a light receiving use optical fiber,

5 the measurement result always contains the pulse wave signals due to heartbeats. Contrary, if the setting of the optical fibers is inadequate, since the inspection light used for the measurement has not sufficiently passed through the blood vessel inside the living body,

10 the measurement result hardly contains the pulse wave signals due to heartbeats, when the setting of the optical fibers is inadequate.

[0026]

In the present invention, the signal components relating to the pulse wave due to heartbeats are extracted via the pulse wave calculation unit 114 from the hemoglobin signal information stored in the memory 109 and the hard disk 111 and through calculation and evaluation of the peak magnitude at the center frequency 20 f_o of the fourth order statistic K_{f_o} with the setting evaluation unit 115, the judgment of setting adequacy of the optical fibers is enabled. Since the value of fourth order statistic K_{f_o} under normal distribution is 3, when as the threshold value, for example, 3 is 25 used, it is judged that when the fourth order statistic K_{f_o} is more than 3, the setting of the optical fibers is adequate and when less than 3 the setting is

inadequate. However, the threshold value can be arbitrarily input by an operator via an input unit (not shown).

[0027]

5 Since the judgment of the present invention which uses the magnitude of the value of the fourth order statistic Kfo depends on the amount of inspection light used for the measurement passed through inside the living body, the case (Fig.2) in which the setting of
10 the optical fibers is adequate and the case (Fig.5) in which the optical fibers are inadequately remote from the surface of the living body representing the measurement object can be discriminated. Further at the same time, the judgment of the present invention, which
15 uses the magnitude of the value of the fourth order statistic Kfo can discriminate between the case (Fig.2) in which the setting of the optical fibers is adequate, the case (Fig.3) in which setting of the irradiation use optical fiber is inadequate and the case (Fig.4)
20 in which setting of the light receiving use optical fiber is inadequate.

[0028]

Now, a specific example of hemoglobin signal processing according to Fig.6 embodiment will be
25 explained. By making use of Figs.7~9 a case when a setting of an optical fiber is adequate will be explained. Fig.7 shows a measurement result of one

channel for the optical measurement for living body, which is the result according to step 601 in Fig.6 flowchart. Fig.8 is a processed result in which the processing in Fig.6 step 602,in that the HPF (High frequency band Pass Filter) is applied to the measurement result of one channel for the optical measurement for living body as shown in Fig.7. Fig.9 is a processed result in which the processing in Fig.6 step 603,in that the frequency analysis is performed to the measurement result of one channel for the optical measurement for living body as shown in Fig.8. According to the processed result as shown in Fig.9, from signals in the frequency band representing the pulse wave components due to the heartbeats the frequency having the maximum power is detected as the center frequency f_o . Since the present example is a measurement result of a newborn, a center frequency (901) of 1.9Hz is detected among the frequency band signals of 1.6~2.1Hz.

{0029}

Since the fourth order statistic K_{f0} determined by making use of the center frequency f_o is 7.43, when the threshold value 3 is used which is the value of fourth order statistic K_{f0} under normal distribution, the measurement result of the present example contains a substantial amount of pulse wave signals and the setting of the optical fibers is judged as adequate. Further, in an example when the subject is an adult, 0.8~1.2 Hz

is used as a frequency band representing pulse wave due to heartbeats.

[0030]

By making use of Figs.10~12 a case when a setting 5 of an optical fiber is inadequate will be explained. Fig.10 shows a measurement result of another channel than that of Fig.7 for the optical measurement for living body in an example when the subject is a newborn and which is the result according to step 601 in Fig.6 10 flowchart. Fig.11 is a processed result in which the processing in Fig.6 step 602,in that the HPF (High frequency band Pass Filter) is applied to the measurement result of one channel for the optical measurement for living body as shown in Fig.10. Like 15 the processing used in Fig.8, the frequency component used for the HPF is, for example, 1Hz in an example when the subject is a newborn. Fig.12 is a processed result in which the processing in Fig.6 step 603,in that the frequency analysis is performed to the measurement 20 result of one channel for the optical measurement for living body as shown in Fig.11. According to the processed result as shown in Fig.12, from signals in the frequency band representing the pulse wave components due to the heartbeats the frequency having 25 the maximum power is detected as the center frequency f_o . Since the present example is a measurement result of a newborn, a center frequency (1201) of 1.8Hz is

detected among the frequency band signals of 1.6~2.1Hz.

[0031]

Since the fourth order statistic Kfo determined by making use of the center frequency fo is 2.74, when 5 the threshold value 3 is used which is the value of fourth order statistic Kfo under normal distribution, the measurement result of the present example contains no substantial amount of pulse wave signals and the setting of the optical fibers is judged as inadequate.

10 [0032]

Figs.13~15 are flowcharts for explaining respective sequences of optical measurement for living body of embodiments of optical measurement apparatus for living body according to the present invention 15 provided with a setting adequacy evaluation and judgment function of the irradiation use optical fibers and/or the light receiving use optical fibers of which function has been explained with reference to Fig.6 flowchart.

20 [0033]

In Fig.13 embodiment, at first in step 1301, optical fibers are set on the body surface in the inspection area of the subject, subsequently, in step 1302 a short time preparatory measurement of about 10 25 seconds is performed. Then, in step 1303, by making use of the preparatory measurement at step 1302 the evaluation and judgment according to Fig.6 on the

setting adequacy of the optical fibers is performed for respective measurement channels, and when there are measurement channels of which setting are judged inadequate, the process returns to step 1301, the 5 optical fibers of the measurement channels of which setting are judged inadequate are reset, the steps 1302 and 1303 are repeated, and when no measurement channels of inadequate setting is reached, the process advances to step 1304 of an actual measurement.

10 [0034]

In Fig.14 embodiment, at first in step 1401 like step 1301 in Fig.13, optical fibers are set on the body surface in the inspection area of the subject, and omitting the preparatory measurement in Fig.13, at step 15 1402 the actual measurement is directly performed. After completing the actual measurement, at step 1403, by making use of the actual measurement at step 1402 the evaluation and judgment according to Fig.6 on the setting adequacy of the optical fibers is performed for 20 respective measurement channels, and the measurement data of measurement channels of which settings are judged adequate are accepted as hemoglobin signals to be used for obtaining living body information inside the living body which is the primary target of the 25 optical measurement for living body at step 1404 and on the other hand, the measurement data of measurement channels of which settings are judged inadequate are

rejected as hemoglobin signals to be used for obtaining living body information inside the living body which is the primary target of the optical measurement for living body at step 1405 by a rejecting means.

5 [0035]

Fig.15 is a combination of concepts of the measurement sequences of Figs.13 and 14, at first in step 1501, optical fibers are set on the body surface in the inspection area of the subject, subsequently, 10 in step 1502 a short time preparatory measurement of about 10 seconds is performed, then, in step 1503, by making use of the preparatory measurement at step 1502 the evaluation and judgment according to Fig.6 on the setting adequacy of the optical fibers is performed for 15 respective measurement channels, and when there are measurement channels of which setting are judged inadequate, a simple resetting work such as moving the entire probe a little is performed, and the steps 1502 and 1503 are repeated, and the settings are reached 20 mostly OK, the process advances to step 1504 of an actual measurement. This is for the purpose of avoiding useless long time restriction of the subject by repeating the optical fiber resetting, the preparatory measurement and the setting adequacy evaluation of the optical 25 fibers. After the above process, the measurement data of measurement channels of which settings are judged adequate at the last preparatory measurement are

accepted as hemoglobin signals to be used for obtaining living body information inside the living body which is the primary target of the optical measurement for living body at step 1505 and on the other hand, the 5 measurement data of measurement channels of which settings are judged inadequate are rejected as hemoglobin signals to be used for obtaining living body information inside the living body which is the primary target of the optical measurement for living body at 10 step 1506 by a rejecting means. According to Fig.15 method, even when a setting fault of an optical fiber is caused during the actual measurement, the measurement data from the optical fiber at which the fault is caused are prevented from being accepted as 15 data for obtaining the living body information inside the living body of the subject.

[0036]

Further, any of the sequences of the optical measurement for living body according to Figs.13~15 can 20 be used depending on the condition of the subject.

[0037]

The present invention is not limited to the above embodiments and can be carried out in a variety of modifications in a range without departing the gist of 25 the present invention. In particular, although the number of the fiber units 103 which guide and irradiate laser beams to the scalp portion and of the fiber units

103' which receive and detect the reflected near infrared light are not explained in the present embodiments, the number thereof is of course can be either single or plural.

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